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Modeling the drug release from HPMC tablets with different macrostructure

Master thesis in: Transport Phenomena

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Part of this work has been performed in partnership with the Chalmers University of Technology in Goteborg, under the supervision of Prof. Anette Larsson.

To my mam and dad

Questo testo è stato stampato in proprio, in (font adoperato)

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Abstract

Using 3D printing, it is possible to design and develop complex dosage forms that can be suitable for tuning drug release. It, indeed, allows a flexible variation of the drug dose, release characteristics, or implementation of combinations of several drugs in the same dosage form to correspond to the individual patient needs. Polymers are the key materials that are necessary for 3D printing and it is important to understand which polymers are suitable for extrusion-based 3D printing of pharmaceuticals.

With 3D printer disc with different infill, disc with different pattern of infill and disc with different macrostructure can be printed. Discs with different macrostructure have been studied in order to analyze how different macrostructure impact on the drug release.

When a network of long polymers is immersed in a physiological fluid, this starts to penetrate inside the polymeric hydrophilic matrix. When a certain solvent concentration is reached, the polymeric chains unfold due to a glass-rubber transition, and a gel layer is formed. In the swollen region, the drug molecules can diffuse toward the dissolution medium, once they are dissolved.

In order to consider the hydrogel mechanics, the pure hydrogel behavior has been studied. Hydrogels normally couple solvent mass transport to system deformation and vice versa. This phenomenon is generally called poroelasticity and it is characteristic also of other materials. This complex behavior, generally defined "poroviscoelastic", is the sum of a poroelastic and a viscoelastic behavior. The first is due to long-range motion of the water molecules, which can enter (swelling) or leave (shrinking) the system or move within the system (isochoric deformation). The viscoelasticity, instead, is mainly a characteristic of the polymeric structure, which can rearrange its spatial configuration (i.e. by the breakage and reformation of cross-links) and respond with a time dependent mechanical behavior. The full understanding of this behavior is crucial to correctly design such complex systems.

The aim of this thesis is to simulate thought poroelastic modeling, the drug release from tablets of HPMC hydrogel with different macrostructures that will be printed using 3D printer. In this thesis, the monophasic approach, which is more consistent, has been chosen. This model considered hydrogel as single-phase matter, in which several components can coexist and therefore the properties are not of the single phase but of the combination of all the species.

The simulation has been done with the software COMSOL Multiphysics 5.2. This software is able to resolve the Partial Different Equations (PDEs) that describe the system, through the Finite Element Method (FEM). The work can be divided in two parts. In the first part the mathematical models of the tablet with different macrostructure have been studied and implemented in the software, at this point the sweep parametric has been executed in order to understand how the parameters impact system.

In the second part, since different models have been studied, the comparison between them has been done in order to understand how the macrostructure impacted the system.

References

- 1. Zhang, J; Feng, X; Patil, H; Tiwari, R; Repka,M, Coupling 3D printing with hot-melt extrusion to produce controlled-release tablets, Journal of Pharmaceutical Sciences, 186 (2016).
- 2. Zhanga, J; Yangb, W; Anh Q. Voa, Fenga, X; Yea, X; Kima, D; Repka, M, Hydroxypropyl methylcellulose-based controlled release dosage by melt extrusion and 3D printing: Structure and drug release correlation, Carbohydrate polymers, 177(2017).
- 3. Solanki; Tahsin, Md; Shah, A; Serajuddin, A, Formulation of 3D Printed Tablet for Rapid Drug Release by Fused Deposition Modeling: Screening Polymers for Drug Release, Drug-Polymer Miscibility and Printability, Journal of Pharmaceutical Sciences, 107 (2018).
- 4. Patil, H; Tiwari, R; Repka, M; Hot-Melt Extrusion: from Theory to Application in Pharmaceutical Formulation, PharmSciTech,17(2016).
- 5. Repka, M; Shah, S; Lu, j; Maddineni, S; Morott, J, Melt extrusion: process to product, Expert Opin, Drug Deliv,9(2012).
- 6. Azad, M; Olawuni, D; Kimbell, G; Badruddoza, A; Hossain, S and Sultana, T, Polymers for Extrusion-Based 3D Printing of Pharmaceuticals: A Holist Materials-Process Perspective, Pharmaceutics,12(2020).
- Aho, J.; Bøtker, J. P.; Genina, N.; Edinger, M; Arnfast, L.; Rantanen, J; Roadmap to 3D-Printed Oral Pharmaceutical Dosage Forms: Feedstock Filament Properties and Characterization for Fused Deposition Modeling, Journal of Pharmaceutical Sciences, 108 (2019).
- 8. Zhanga, J; Fenga, X; Patil, H; Tiwari, R; Repka, M, Coupling 3D printing with hot-melt extrusion to produce controlled-release tablets, International Journal of Pharmaceutics 519 (2017).
- 9. Melocchi, A; Parietti, F; Maroni, A; Foppoli, A; Gazzanica, A; Zema, L, Hotmelt extruded filaments based on pharmaceutical grade polymers for 3D printing by fused deposition modeling, International Journal of Pharmaceutics 509 (2016).

- Goyanes, A; Buanz, A; Basit, A; Gaisford, S, Fused-filament 3D printing (3DP) for fabrication of tablets, International Journal of. Pharmaceutics,476(2014).
- 11. Goyanes, a; Buanz, A; Hatton, G; Gaisford, S; Basit, 3D printing of modified-release aminosalicylate (4-ASA and 5-ASA) tablets,Eur J Pharm Biopharm,89(2015).
- 12. Kadrya, H; Hilala, T; Alama, K; Joyc, C; Ahsan, F; Multi-purposable filaments of HPMC for 3D printing of medications with tailored drug release and timed-absorption, International Journal of. Pharmaceutics,544(2018).
- 13. Caccavo, D; Cascone, S, Lamberti, G; Barba, A.A. ; Larsson, A, Swellable Hydrogel-based Systems for controlled Drug Delivery, in Smart drug delivery system, INTECH(2016).
- 14. Caccavo, D; Vietri, A; Lamberti, G; Barba, A.A; Larsson, A, Modeling the mechanics and the transport phenomena in hydrogels, Chapter 12
- 15. Siepmann, J; Peppas, N.A.; Modeling of drug release from delivery systems based on hydroxypropyl methylcellulose (HPMC), Advanced drug delivery reviews,48(2001).
- 16. Caccavo, D; Lamberti, G; Barba, A.A, Mechanics and drug release from poroviscoelastic hydrogels: Experiments and modeling, European Journal of Pharmaceutics and Biopharmaceutics, 152(2020).
- 17. Caccavo, D; Cascone, S; Lamberti, G and Barba, A.A, Hydrogels: experimental characterization and mathematical modelling of their mechanical and diffusive behavior, Royal society of Chemistry (2018).
- 18. Caccavo, D, Analysis and modeling of the behavior of hydrogels-based systems for biomedical and agro-food applications (PhD Thesis).
- 19. Gurtin, M. E., Fried, E., & Anand, L, The mechanics and thermodynamics of Continua, New York: Cambridge University Press (2010).
- 20. Caccavo, D; Lamberti, G; PoroViscoElastic model to describe hydrogels' behavior, Material science and engineering:C,76(2017).
- 21. FLORY, P. J. Principles of Polymer Chemistry, Cornell University (1953)
- 22. Lucantonio, A; Nardinocchi, P; and Teresi, Multiphysics Modeling of Swelling Gels (2012)
- 23. Bajwa, G.S; Sammon, C; Timmins, B; D. Melia, C; Molecular and mechanical properties of hydroxypropyl methylcellulose solutions during the sol: gel transition, Polymer,50 (2009)
- 24. Chen, H.H; Rheological properties of HPMC enhanced Surimi analyzed by small- and large-strain tests: I. The effect of concentration and temperature on HPMC flow properties, Food hydrocolloids,22 (2008)

- 25. Sinko, C; P. Smith, D and R. Nixon, P ,Mechanical characterization of hydroxypropyl methylcellulose:modulus determination from indentation loading profiles, International Journal of Pharmaceutics,81(1992)
- 26. Qijun Li a, Haoyang Wen a, Danyang Jia c, Xiaoying Guan a, Hao Pan d, Yue Yang a, Shihui Yu a, Zhihong Zhu a, Rongwu Xiang b, *, Weisan Pan, Preparation and investigation of controlled-release glipizide novel oral device with three-dimensional printing, International Journal of Pharmaceutics,525(2017)

Eventuali ringraziamenti (su pagina dispari)

Aggiungere in fine una pagina (pari) completamente bianca